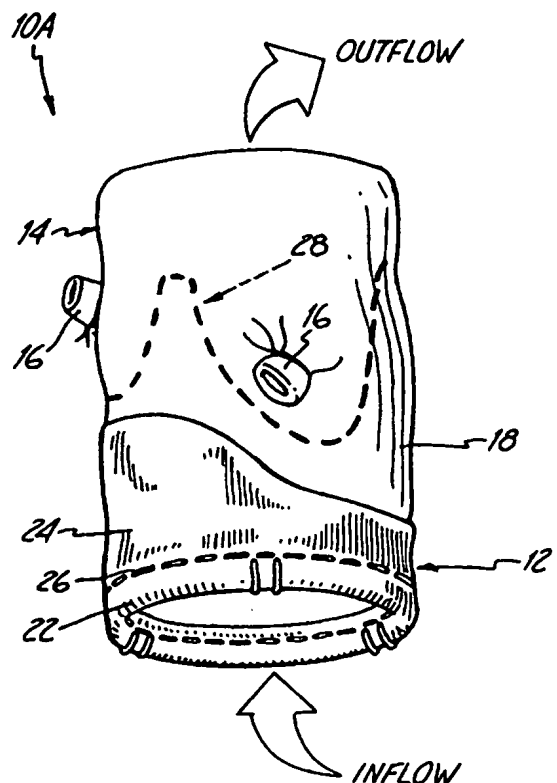


PCT

WORLD INTELLECTUAL PROPERTY ORGANIZATION
International Bureau



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

<p>(51) International Patent Classification ⁶ : A61L 27/00, A61F 13/02, A61B 17/11, A61F 2/16, 2/06, 2/24</p>	<p>A1</p>	<p>(11) International Publication Number: WO 98/29146 (43) International Publication Date: 9 July 1998 (09.07.98)</p>
<p>(21) International Application Number: PCT/US97/23874 (22) International Filing Date: 31 December 1997 (31.12.97) (30) Priority Data: 08/775,821 31 December 1996 (31.12.96) US (71) Applicant: ST. JUDE MEDICAL, INC. [US/US]; One Lillehei Plaza, St. Paul, MN 55117 (US). (72) Inventors: HEALY, Steven, J.; 4155 Primrose Path, Vadnais Heights, MN 55127 (US). SCHROEDER, Richard, F.; 4675 Gershwin Avenue, Oakdale, MN 55128 (US). (74) Agents: CHAMPLIN, Judson, K.; Westman, Champlin & Kelly, International Centre, Suite 1600, 900 Second Avenue South, Minneapolis, MN 55402 (US) et al.</p>		<p>(81) Designated States: BR, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published With international search report.</p>
<p>(54) Title: INDICIA FOR PROSTHETIC DEVICE</p> <p>(57) Abstract</p> <p>A prosthetic stentless aortic tissue valve (10A) includes a substantially annular valve body (12) having a leaflet (34) carried therein for occluding blood flow therethrough. A root (14) extends generally coaxially from the valve body (12). Visual markings (28) are provided on the root and act as a sculpting guide for a surgeon during implantation of the prosthetic heart valve (10A) to sculpt portions of sinus areas of the root.</p> 		

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

-1-

INDICIA FOR PROSTHETIC DEVICE

FIELD OF THE INVENTION

This invention relates generally to implantable bioprosthetic devices, and more particularly is directed to implantable products to repair or replace the valves of the heart.

BACKGROUND OF THE INVENTION

Prosthetic heart valves are used to replace diseased natural heart valves. Several categories of prosthetic heart valves are in existence. In prosthetic heart valves, one or more leaflets or occluders are carried within an annulus of the prosthesis and act as a valve to blood flow. The leaflet may be of a biological material or a synthetic material for bioprosthetics or, in a mechanical prosthesis, may be of a biocompatible material such as pyrolytic carbon.

One type of bioprosthetic heart valve is a stentless aortic tissue valve. Such tissue valves include a root version and a sub-coronary version. The root version includes an aortic root which is used to replace a diseased aortic root of a patient. However, in instances where the natural aortic root (or aortic arch) is healthy, the sub-coronary version may be used and the native root can be left intact.

In many instances, the surgeon will excise (or "sculpt") portions of the sinus areas of the prosthetic aortic root of the root version stentless aortic tissue valve to form a sub-coronary prosthesis. Often, this procedure must be done during surgery when operative time is limited. It is difficult to accurately sculpt the sinus areas and avoid damage to the leaflets due to lack of visibility of the inside of the heart valve. Currently, stentless aortic roots have been provided

-2-

which include markings to aid in modifying the device from a full root replacement to a sub-coronary application. However, these markings are of only marginal assistance to the surgeon. One bioprosthetic
5 stentless aortic root uses very unrefined surface indicators formed by sutures which are sutured through the tissue. Another stentless aortic root requires the surgeon to rely on sketches which are provided in surgical literature.

10 For other bioprosthetic devices, such as a valved conduit, the device must be oriented and implanted correctly with respect to blood flow direction. Still other bioprosthetic devices, such as pericardial patches, may require that the device be
15 oriented and implanted in a particular manner. For example, it may be desirable to implant the patch so that the strongest axis of the device is aligned with the major stress axis. Other bioprosthetic devices, such as stentless mitral valves or mitral valve repair
20 kits can be scaled (cut down) for a proper fit while maintaining proper geometry. Further, annuloplasty rings must be of the correct size for valve repair.

SUMMARY OF THE INVENTION

 Accordingly, it is a general aim of the
25 present invention to provide a new method and apparatus for sculpting a bioprosthetic implant, such as a bioprosthetic root of a stentless aortic valve prosthesis or providing directional indicators or other information to biological prostheses such as a
30 pericardial patch, valved conduit, etc. The prosthesis includes a marking or visual guide for excising portions of the prosthesis or instructions for use of the prosthesis, such as the direction or position of the prosthesis relative to implant position. In one

-3-

embodiment, a prosthetic stentless aortic tissue valve comprises a substantially annular valve body which includes at least one leaflet or other type of occluder carried therein for occluding blood flow through the valve body. An aortic root extends from the valve body and is generally coaxial with the valve body. A visual marking is provided on the root and provides a sculpting guideline for use by a surgeon during implantation of the prosthetic heart valve to trim the root. The marking indicates portions of sinus areas of the root which are removed to create a sub-coronary prosthetic stentless aortic valve. In one embodiment, the visual marking generally conforms to the leaflet of the bioprosthetic heart valve. The marking may be formed by any appropriate means, including a biocompatible dye or laser markings.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a side perspective view of a prosthetic stentless aortic tissue valve in accordance with the present invention.

Figure 2 is a side perspective view of the valve of Figure 1 following excision of portions of the prosthetic aortic root shown in Figure 1.

Figure 3 is a cross-sectional view of the root valve of Figure 1 showing leaflets carried therein.

Figure 4 is a plan view of a pericardial patch in accordance with one embodiment of the invention.

Figure 5 is a perspective view of a vascular graft or nerve channel in accordance with one embodiment of the invention.

Figure 6 is a perspective view of a valved conduit in accordance with one embodiment of the invention.

-4-

Figure 7 is a plan view of an annuloplasty ring in accordance with one embodiment of the invention.

Figure 8 is a perspective view of an anterior mitral valve repair leaflet or cusp in accordance with one embodiment of the invention.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

The present invention provides indicators on bioprosthetic devices to aid in their implantation. Such indicators provide a number of advantages. These advantages include that the indicators allow the surgeon to tailor each device to the specific physiology of the patient. The devices can also be used for multiple purposes in that the device may be modified for various applications of the device. Furthermore, such indicators allow the device to be accurately oriented to optimize results of the use of the device. In addition, the indicators do not affect the integrity or durability of the device.

Figure 1 is a side perspective view of a bioprosthetic stentless aortic root valve 10A in accordance with the present invention. Valve 10A includes a valve body portion 12 and an aortic root portion 14. Root 14 includes remnant coronary ostia 16. Valve body 12 includes a commissure support portion 18, annular orifice 22, reinforcement material 24 and sutures 26 which attach material 24 to annular orifice 22. Reinforcement material 24 could be, for example, a non-absorbable polymer, such as a polyester, polytetrafluoroethylene, or nylon, pericardium tissue, a resorbable polymer, such as polylactic acid (PLA) or polyglycolic acid (PGA), or a semi-rigid thin stent. Material 24 may also be coupled to root 14 using an adhesive.

-5-

As shown in Figure 1, root valve 10A includes visual marking 28 on root valve 10A which generally divides root 10A into two portions, valve body 12 and root 14. Remnant coronary ostia 16 are carried on the root 14. Visual marking 28 generally conforms to the profile of the leaflets (not shown in Figure 1) carried within valve body 12.

Valve 10A as shown in Figure 1 is adapted for replacement of the full natural aortic root of a patient. However, during the surgical operation, if the surgeon discovers that the natural aortic root or aortic arch is healthy, the surgeon may decide to leave the natural root intact and implant a sub-coronary valve replacement within the aortic arch. Typically, a sub-coronary valve will provide enhanced hemodynamics, long term durability and reduced surgical complexity and is therefore preferable to the root version.

The present invention allows the surgeon to quickly and efficiently modify tissue valve 10A as shown in Figure 1 by removing root 14 to form sub-coronary tissue valve 10B shown in Figure 2. The portions 12, 14 for subcoronary implants may be separated immediately prior to implantation, or during the implant procedure if full root is used. As shown in Figure 2, root 14 has been removed, utilizing standard surgical implements (scissors, scalpels, etc.) at visual marking 28, leaving cut line 30 on the outflow edge of valve 10B. Thus, tissue valve 10B is now adapted for sub-coronary implantation into the natural aortic root of the patient. This modification could be performed on either one, two or three of the coronary sinuses, depending on the surgeon's preferences.

Visual marking 28 is preferably formed during manufacture of valve 10A and preferably provides an

-6-

optimal, or near optimal sculpting indicator for each individual valve. Specifically, visual marking 28 is positioned above and closely follows the shape and contour of leaflets 34 shown in Figure 3 which are carried in valve body 12. Figure 3 is a cross-sectional view of valve 10A and shows the relationship between visual marking 28 and leaflets 34. It is important in stentless aortic valves that marking 28 is placed in a consistent fashion in relation to the point of leaflet attachment in order to assure proper valve function. Marking 28 can be formed from any suitable biocompatible material which will be visible by the surgeon during surgery. For example, marking 28 may be formed of toluidine blue dye or other organic biocompatible dyes. In another embodiment, a laser may be used to form visual marking 28. The energy output, wavelength and duration of such laser should be selected such that valve 10A is not damaged during the marking procedure. Preferably, visual marking 28 is applied prior to packaging and shipping of valve 10A. The visual markings of the present invention do not damage the bioprosthesis or affect the functioning of the prosthesis.

Marking 28 may be applied manually by visually inspecting valve body 12 and the position of the leaflets. Further, a template may be used to apply visual marking 28. A machine may also be employed to apply marking 28 in which the machine follows a template stored in a computer memory. Additionally, such machine may include a sensor such as an ultrasonic sensor, a laser indicator, a contact measuring device, MRI, etc., which is capable of locating the position of leaflets within valve 10A and responsively controlling application of marking 28 to enhance the precision of

-7-

the application of marking 28. In another embodiment, a polymer, which may be colored, such as a fabric, or other visual markers are adhered using biocompatible biological or synthetic adhesives to the surface of the device, or the adhesive itself could be colored, indicating where the tissue should be excised, such as along marking 28 of Figure 1, or may even include a part of or the entire region between marking 28 and orifice 22.

One aspect of the present invention is that the visual markings do not damage the device. One important concern with bioprosthetic devices is that of mineralization. Mineralization refers to a process in which the material of the device becomes inflexible and brittle due to the incorporation of calcific deposits. Research indicates that one cause of mineralization is abnormal stress concentrations in the tissue. For example, puncturing the surface of the device, such as with sutures, can cause focal stress concentration. Thus, one aspect of the present invention is that the visual markings do not damage the tissue matrix of the device.

It will be understood that the invention may be used with other types of prostheses. For example, Figure 4 is a plan view of a pericardial patch 50 in accordance with the invention. The material of patch 50 is typically stronger in the direction of the major fiber orientation. In surgical cases where stress is a factor, it is preferable to use a patch device aligned along the axis of stress. It is within the contemplation of this invention to put a directional indicator, such as an arrow, to indicate the direction of the strong axis of the patch 50, or a written use direction to indicate, for example, which is the smooth

-8-

or rough side of the patch 50, or the size of the patch 50.

For blood flow conduits comprising a biological or synthetic material, such as a mechanical or biological valved graft 52 shown in Figure 6 or vascular graft 54 shown in Figure 5, blood flow directional indicators or size indicators may be placed on the device to assure that the device is oriented and implanted correctly with respect to blood flow direction. This allows the surgeon to identify the distal and proximal end, conduit size, appropriate valve size and position within the conduit, etc. Such markings are preferably applied prior to surgery, preferably during manufacture.

An annuloplasty ring 56 shown in Figure 7, also in accordance with the present invention, provides sizing directions, modification indicators, such as a cut line indicator, and/or placement orientation instructions. This is particularly useful for annuloplasty rings that have variable stiffness around the ring circumferences such as anteriorly or posteriorly or are of designs such that material or geometric properties have importance with regard to implant orientation. For example, in order to improve the healing response of ring 56, cell adhesion proteins may be placed on the surface of the device that contact the mitral annulus.

Additionally, the invention is applicable to stentless mitral valves as well as mitral valve repair kits. Indicators are placed on the valves or individual leaflets as shown in Figure 8 to allow the surgeon to sculpt the valve proportionately in relation to annulus size for improved valve function. In the case of a full mitral valve replacement, this anterior cusp, shown in

-9-

Figure 8, as well as a similar posterior cusp would be combined to form a complete valve. Both of these segments, however, could still be subject to sculpting. This is particularly useful in allowing the surgeon to
5 alter the device with respect to annular geometry as well as length of papillary attachment. In the case of mitral repair kits, each leaflet may have proportional sculpting indicators for the same purpose. This assures that the leaflets are scaled to size with respect to all
10 dimensions and that they are placed in the correct position (anterior or posterior).

Nerve channels may also be made in accordance with the invention where implant orientation and sizing of the nerve channel are important to the success of the
15 device. Figure 5 is an example of a nerve channel that could be sized appropriately for the intended use, i.e., reduced diameter and length. In addition, ligament replacements could be marked to include sizing information as well as implantation orientation.

As shown and described herein, the invention includes placing indicia on a surface of a prosthetic device. This indicia is applied to a flexible layer of the device, such as shown in the examples set forth herein. The indicia is applied in a manner which does
20 not stress the material to an extent which would damage the material or could lead to mineralization. The indicia is used during the implantation procedure to provide the surgeon or attending staff with information which will aid in the procedure. This simplifies the
25 implantation process. Further, because the information is more readily apparent, the implantation procedure may proceed at a faster rate thereby shortening the length of time needed to perform the surgery. Thus, the
30

-10-

invention provides more accurate implantation which requires a shortened surgical procedure.

Although the present invention has been described with reference to preferred embodiments,
5 workers skilled in the art will recognize that changes may be made in form and detail without departing from the spirit and scope of the invention. For example, the visual marking may be formed by any appropriate technique and may comprise a plurality of individual
10 markings or may use color as an indicator. The visual marking is applicable to any bioprosthetic or synthetic replacement or repair device for heart valves or other types of implants.

-11-

WHAT IS CLAIMED IS:

1. A prosthetic device for replacing or repairing natural tissue of a patient, comprising:
a flexible layer of a biocompatible material having a surface; and
indicia carried on the surface of the flexible layer wherein the indicia does not damage the material to an extent which would adversely affect the functionality of the material.
2. The prosthetic device of claim 1 wherein the flexible layer is part of a stentless aortic valve and the indicia provides a sculpting guideline.
3. The prosthetic device of claim 1 wherein the flexible layer comprises a portion of a pericardial patch.
4. The prosthetic device of claim 1 wherein the flexible layer comprises a portion of a valved conduit.
5. The prosthetic device of claim 1 wherein the flexible layer comprises a portion of a vascular graft.
6. The prosthetic device of claim 1 wherein the flexible layer comprises a portion of an annuloplasty ring.
7. The prosthetic device of claim 1 wherein the flexible layer comprises a portion of a stentless mitral valve.
8. The prosthetic device of claim 1 wherein the flexible layer comprises a portion of a mitral valve repair leaflet.
9. The prosthetic device of any of claims 1 to 8 wherein the indicia comprises a biocompatible dye applied to the surface of the flexible layer.

-12-

10. The prosthetic device of any of claims 1 to 8 wherein the indicia comprises laser markings formed on the surface of the flexible layer.
11. The prosthetic device of any of claims 1 to 8 wherein the indicia comprises a biocompatible material adhered to the surface of the flexible layer.
12. The prosthetic device of any of claims 1 to 8 wherein the adhesive is colored.
13. The prosthetic device of any of claims 1 to 8 wherein the not damaging of the material reduces mineralization of the material after implantation.

1/8

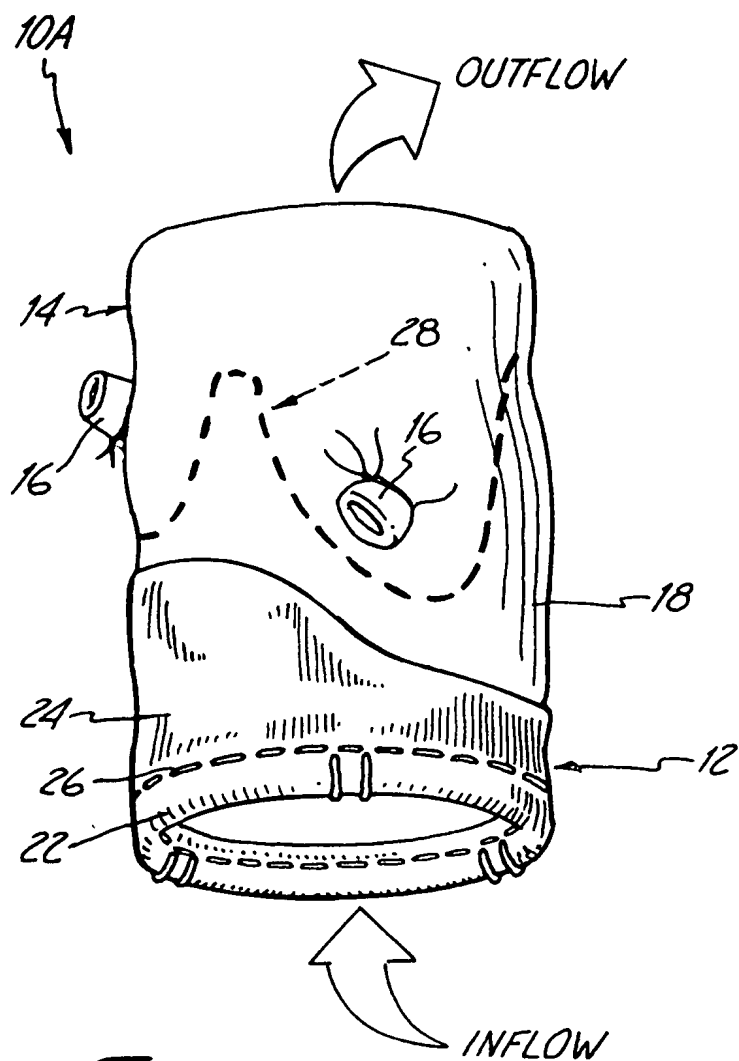


Fig. 1

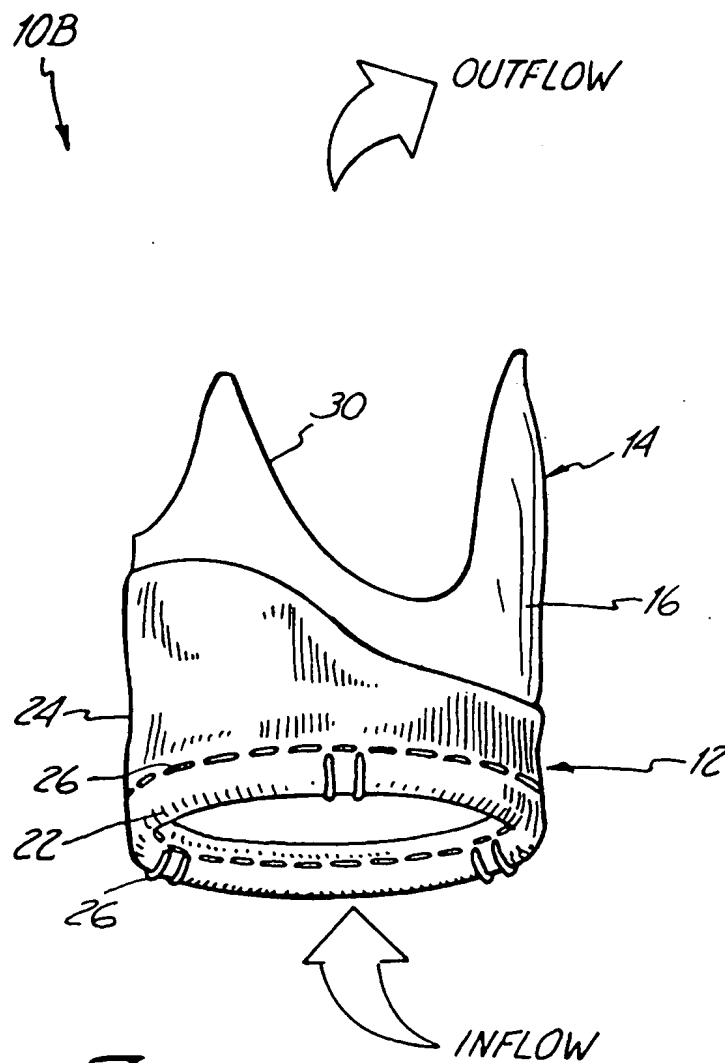


Fig. 2

3/8

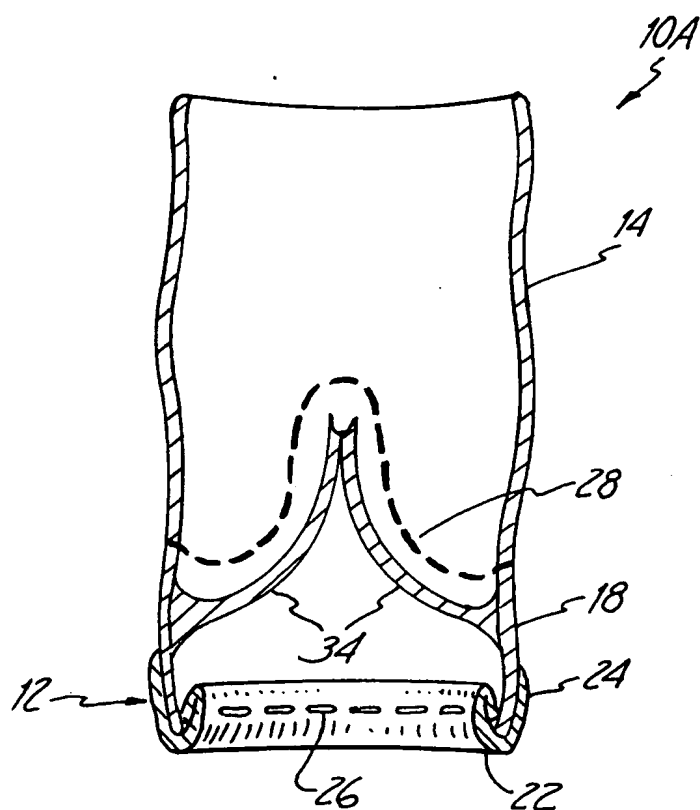
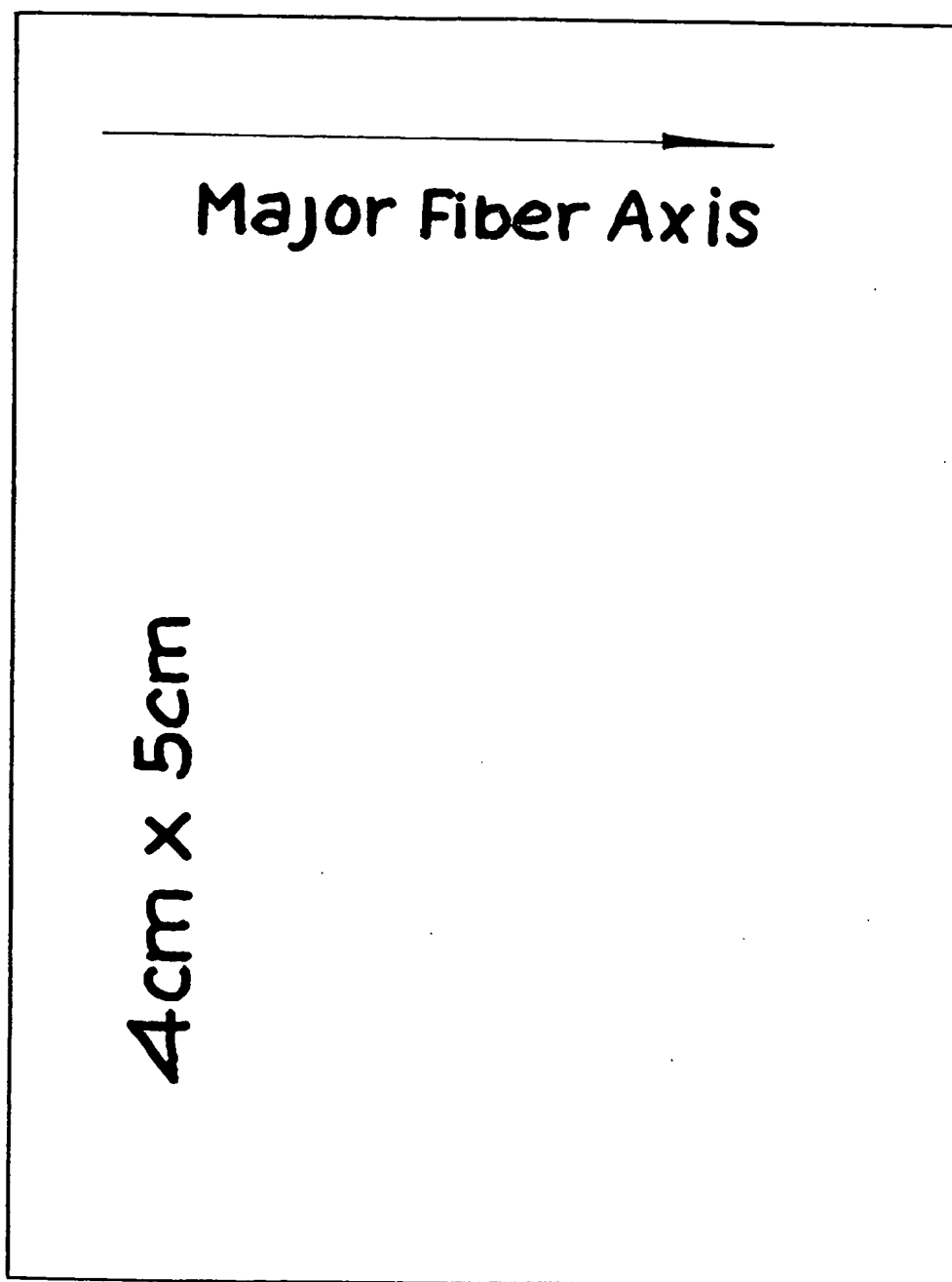


Fig. 3

4/8

Fig. 4



50

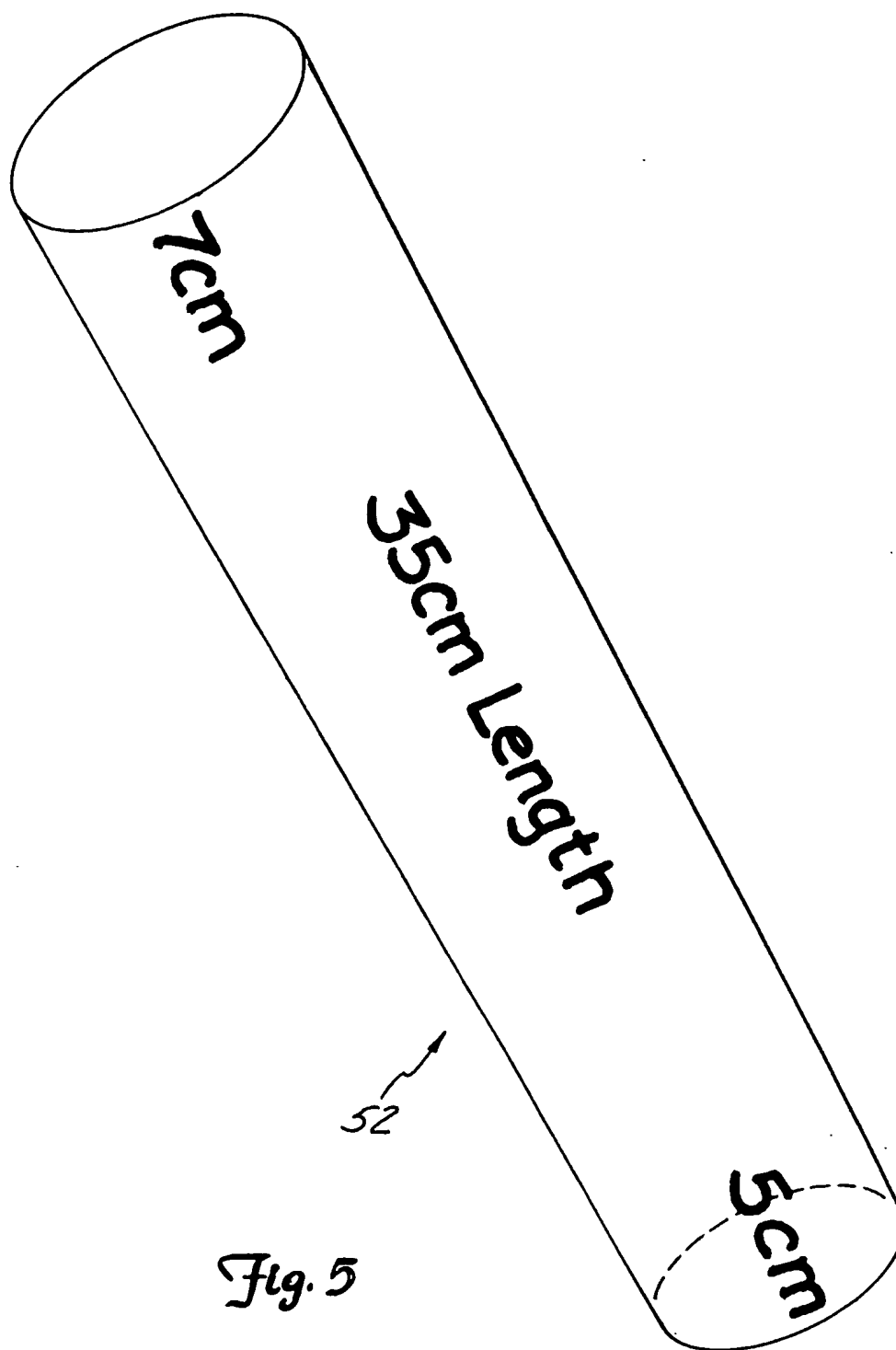
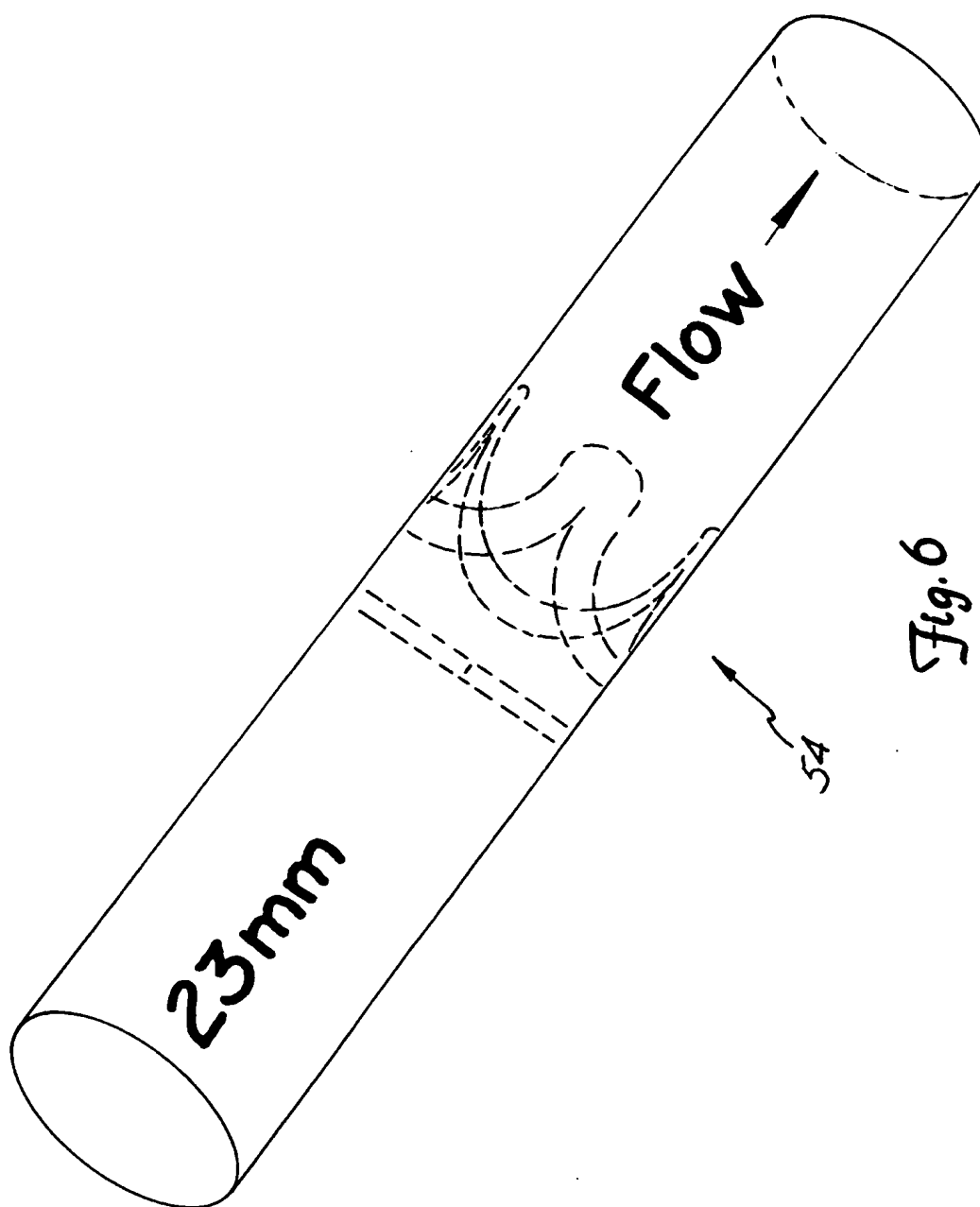
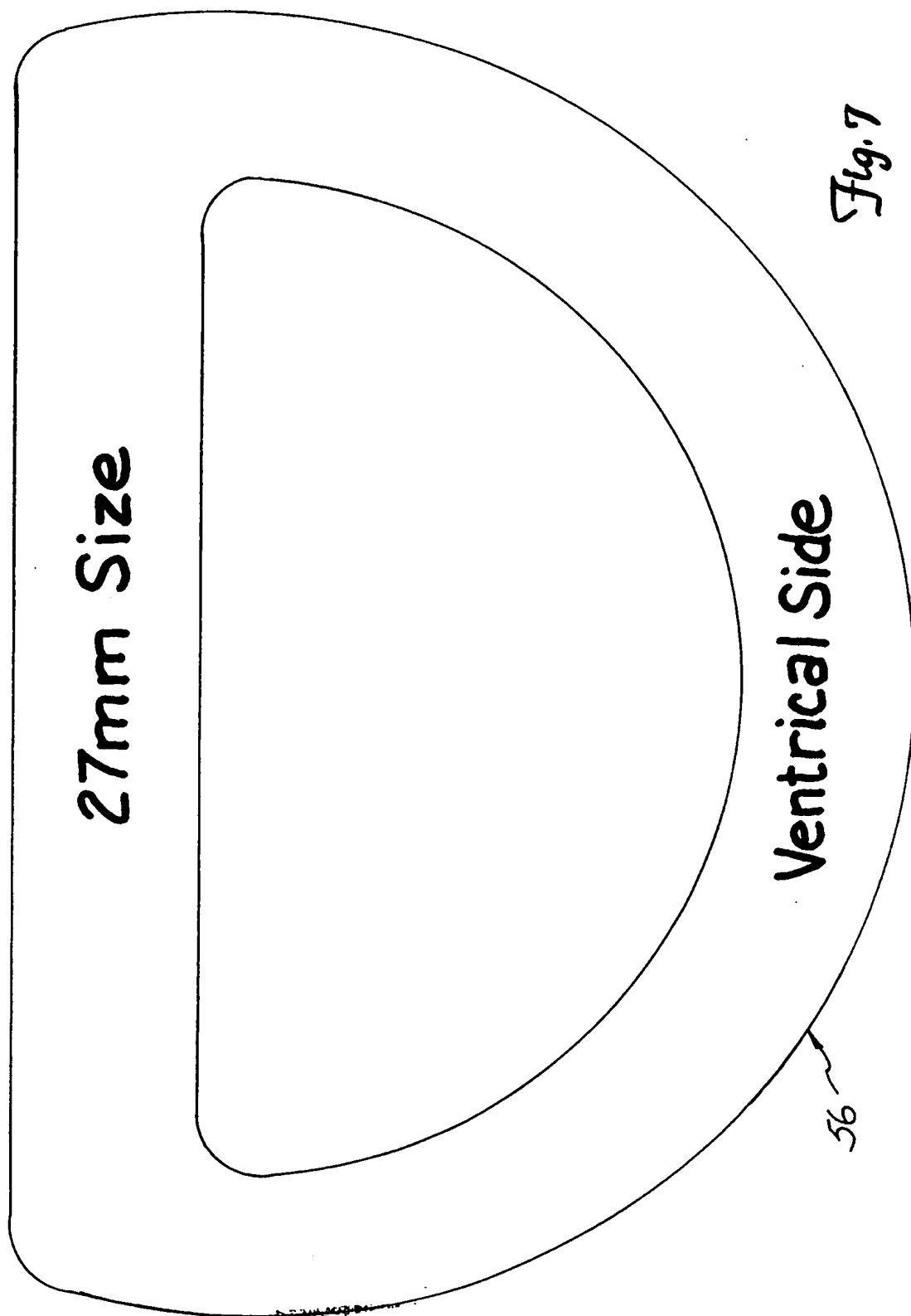


Fig. 5

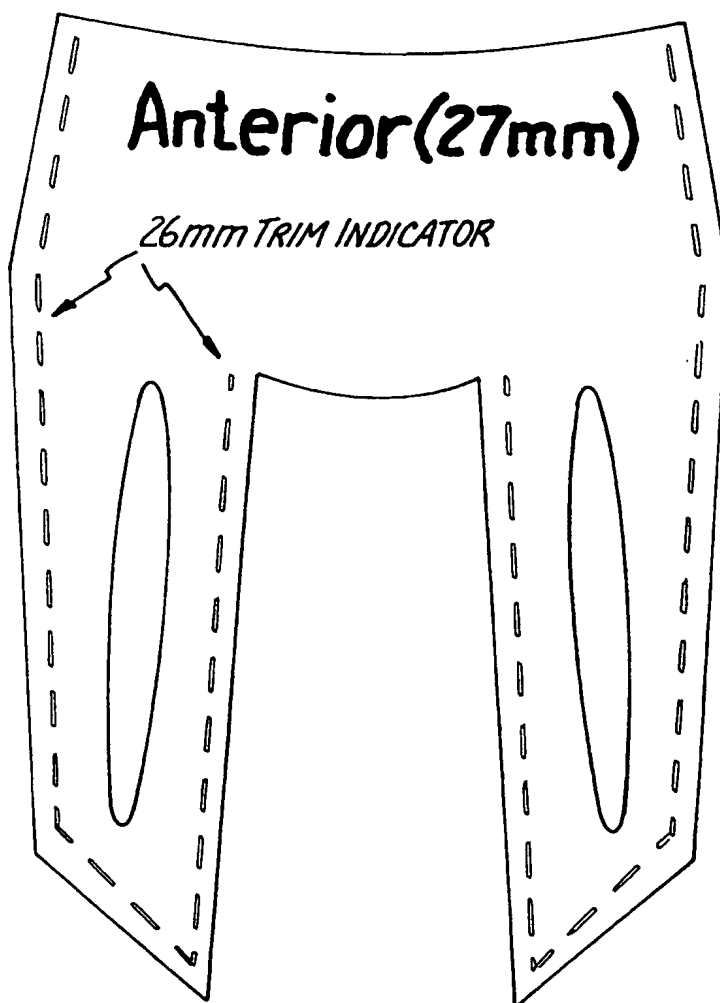


7/8



8/8

Fig. 8



INTERNATIONAL SEARCH REPORT

International Application No.
PCT/US 97/23874

A. CLASSIFICATION OF SUBJECT MATTER

IPC 6 A61L27/00 A61F13/02 A61B17/11 A61F2/16 A61F2/06
A61F2/24

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61L A61F A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 94 04099 A (AUTOGENICS) 3 March 1994 see page 14, line 16-24 see page 35, line 10-23 see page 37, line 22-25 see page 54, line 17-24 ---	1-3,8-10
X	EP 0 699 423 A (MEADOX MEDICALS INC) 6 March 1996 see column 5, line 44 - column 6, line 2 see figures 2,3 A see column 6, line 1 ---	1,5 11
X	US 3 805 301 A (LIEBIG W) 23 April 1974 see column 3, line 3-16 see figure 4 --- -/-	1,5,9

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"Z" document member of the same patent family

Date of the actual completion of the international search

26 March 1998

Date of mailing of the international search report

09.04.98

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl
Fax: (+31-70) 340-3016

Authorized officer

Bichlmayer, K-P

INTERNATIONAL SEARCH REPORT

International Application No.

PCT/US 97/23874

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	EP 0 508 473 A (ENDOASCULAR TECH INC) 14 October 1992 see column 6, line 43-47 ---	11
X	WO 93 15690 A (MEDTRONIC INC) 19 August 1993 see page 18, line 20-23 see page 21, line 3-6 see page 22, line 23-28 see page 24, line 6-20 see figure 2 ---	1,6
X	WO 96 40007 A (PEREDO MARIO O V) 19 December 1996 see page 2, line 23 - page 3, line 14 see page 4, line 18-22 see page 8, line 33-36 see page 9, line 32 - page 111, line 22 see figure 13 ---	1,7
Y	see page 11, line 17-22 ---	13
Y	US 5 509 932 A (KEOGH JAMES R ET AL) 23 April 1996 see column 3, line 39 - column 4, line 2 see column 7, line 20-25 ---	13
X	US 4 586 504 A (DE MEDINACELI LUIS) 6 May 1986 see column 2, line 65 - column 3, line 2 see column 3, line 25-54 see column 4, line 32-43 ---	1,9
X	EP 0 495 417 A (ST JUDE MEDICAL) 22 July 1992 see page 4, column 57, line 3 - page 22 see figure 1 ---	1,6,9
A	US 4 219 721 A (BERNFELD MORRIS ET AL) 26 August 1980 see column 1, line 48-57 see column 2, line 47-64 ---	10
A	US 5 409 472 A (RAWLINGS DAVID A ET AL) 25 April 1995 see column 4, line 12-17 -----	11,12

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 97/23874

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 9404099 A	03-03-94	AU 5014893 A US 5489298 A	15-03-94 06-02-96
EP 0699423 A	06-03-96	AU 1775395 A FI 952213 A JP 8056968 A US 5697970 A	15-02-96 03-02-96 05-03-96 16-12-97
US 3805301 A	23-04-74	CA 995852 A DE 2322611 A FR 2194406 A GB 1383722 A JP 49044591 A	31-08-76 07-02-74 01-03-74 12-02-74 26-04-74
EP 0508473 A	14-10-92	CA 2065634 A,C CA 2202800 A EP 0795305 A JP 6023031 A US 5489295 A US 5609625 A US 5628783 A	12-10-92 12-10-92 17-09-97 01-02-94 06-02-96 11-03-97 13-05-97
WO 9315690 A	19-08-93	US 5201880 A US 5306296 A AU 670934 B AU 3597193 A CA 2127701 A EP 0624080 A US 5674279 A	13-04-93 26-04-94 08-08-96 03-09-93 19-08-93 17-11-94 07-10-97
WO 9640007 A	19-12-96	NONE	
US 5509932 A	23-04-96	NONE	
US 4586504 A	06-05-86	NONE	
EP 0495417 A	22-07-92	US 5064431 A JP 5049655 A	12-11-91 02-03-93
US 4219721 A	26-08-80	NONE	

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 97/23874

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 5409472 A	25-04-95	AT 114958 T	15-12-94
		AU 6045590 A	11-03-91
		CA 2062805 A	04-02-91
		DE 69014888 D	19-01-95
		DE 69014888 T	18-05-95
		EP 0486522 A	27-05-92
		ES 2064747 T	01-02-95
		WO 9101706 A	21-02-91
		GB 2250683 A,B	17-06-92
		JP 5501072 T	04-03-93
		AU 646400 B	24-02-94
		AU 6060390 A	11-03-91
		CA 2058421 A	04-02-91
		EP 0484415 A	13-05-92
		WO 9101707 A	21-02-91
		GB 2248398 A,B	08-04-92
		JP 5501073 T	04-03-93